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## Research Article

Theme: Sterile Products: Advances and Challenges in Formulation, Manufacturing, Devices and Regulatory Aspects

Guest Editors: Lavinia Lewis, Jim Agalloco, Bill Lambert, Russell Madsen, Mark Staples

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# Development of Biotechnology Products in Pre-filled Syringes: Technical Considerations and Approaches

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**Abstract.** A monoclonal antibody (mAb) product development case study is presented to address some of the issues faced during developing a pre-filled syringe (PFS) product for a biotherapeutic. In particular, issues involving incompatibility with silicone oil and a stability-based approach for selection of PFS barrel and tip cap components have been discussed. Silicone spiking studies followed by exposure to agitation stress or accelerated temperature conditions were used to check for incompatibilities of the mAb with silicone oil, a necessary product contact material in PFS. In addition, screening studies to compare various closure materials as well as syringe barrel processing methods were used to select the optimum closure materials as well as the correct syringe processing method. Results indicate that the model mAb formulation used was sensitive to high levels of silicone oil especially under accelerated temperature conditions resulting in formation of protein-silicone particles in the solution for samples that were spiked with the silicone oil. Agitation stress did not have any significant impact on the quality attributes tested. Samples stored in syringe barrels that were processed with sprayed-on silicone had higher levels of subvisible particles as compared to those that were processed with the baked-on process. The tip cap comparability study resulted in one tip cap material having superior compatibility among the three that were tested. The quality attribute that was most impacted by the tip cap materials was mAb oxidation. An approach for evaluation of primary packaging components during the development of pre-filled syringe presentations for biotechnology-based compounds has been highlighted.

**KEY WORDS:** formulation development; PFS; pre-filled syringes; primary container closure system; protein development; silicone oil compatibility; syringe processing; tip cap selection.

## INTRODUCTION

The development of biotechnology products such as therapeutic proteins or vaccines in pre-filled syringes (PFS) has attracted considerable interest from pharmaceutical and biotechnology companies in the past 5 to 7 years. This can be attributed mainly to several benefits that PFS provide including reduction of medical dosing errors, minimized risk for microbial contamination by limiting manipulations prior to dosing, and enhanced convenience and ease of use (1). Pre-filled syringes represent a win-win scenario for end-users as well as manufacturers as they encourage and simplify self-administration by the patient or caregiver and provide reduced therapy and injection cost. A lower “dead volume” in PFS results in a greater number of filled units for a given batch compared to vials hence increasing overall process yield during manufacturing.

In spite of these aforementioned advantages, the development of biotechnology products in PFS presents its own set of distinctive challenges. Most of them are due to the complex and amphiphilic nature of proteins and impact of the container closure on protein stability. Protein stability in PFS over shelf life is a concern due to potential incompatibility of these types of molecules with various contact surfaces and interactions with leachables of the PFS system. Prolonged exposure of these leachables can also increase the potential for various forms of protein degradation including conformational changes, reduced activity, and increased immunogenicity. In addition to protein stability, there are several other technical challenges that are faced by manufacturers including functionality issues (break loose, glide force, and tip cap removal force), filling issues such as “wet plungers”, plunger movement during shipping, and container closure integrity of PFS system.

In this paper, we have highlighted an approach that we used for assessing the suitability of a PFS system for development of a monoclonal antibody (mAb) product. In particular, issues involving incompatibility with silicone oil and a stability-based approach for selection of PFS barrel and tip cap components have been discussed.

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PFS systems essentially consist of a glass barrel made up of type I borosilicate glass that is typically siliconized for syringe functionality (2). Several vendors have the option of a non-glass (plastic) barrel available, but this technology has not attracted a lot of interest and use of glass barrels is still dominant in the industry. Typically during the barrel formation, the glass cane is cut into the required length and formed into the flange end and tip (luer tip). A tungsten pin (other newer metal pins are being explored as well) is used to bore the fluid path through the glass barrel tip. In the case of staked-in needle syringes, once the fluid path is formed by the tungsten pin, a needle is securely placed in that fluid path by means of an adhesive. During this entire process when the tungsten pin is heated to extremely high temperatures, it could form tungsten oxide which in turn can potentially interact with the glass to form complex tungsten polyanions (paratungstenate-A or paratungstenate-B) which could be left behind as tungsten-related residue in the fluid path of the syringes. These residual tungsten polyanions can interact with the protein and lead to further instability issues (3). The amount of residual tungsten polyanion left in the syringe which is available to interact with the formulation is more in the luer-tip syringes compared to the staked-in needle syringes because in the case of the latter, the needle and adhesive minimize the exposed surface area of the actual fluid path to the formulation. Once this fluid path is created, the syringe is further processed for siliconization (followed by baking if required) and washing. Following this, a needle shield (for staked-in needle) or tip cap (for luer slip) is placed on the tip end of the syringe. The overall system is then sterilized and used for fill-finish activities where once filling is completed, a plunger is placed in the syringe and then sent for further finishing operations such as visual inspection, etc.

Based on the above-mentioned process, description, and several literature reports (4–6), the critical parts of the pre-filled syringe system which constitute product contact surface are the glass barrel, elastomeric material used for tip cap/needle shield and plunger, silicone oil (Si-oil) used for siliconization, residual tungsten from boring the liquid path into the tip and the needle, and any residual glue in case of the staked-in needle syringe. Hence, it is important to understand the effect of these contact parts on the stability of protein therapeutics (3).

Although several biotech products such as Enbrel, Prevnar, Epogen, Aranesp, Humira, Pegasys, and Peg-Intron are available in PFS, common approaches taken to develop biotechnology products are not readily available, and there is very little published literature available that describe the issues of protein product development through key approaches and case studies. A few reports on the issues that are faced by the industry during the development of protein therapeutics in PFS, especially shedding light on silicone oil-related issues, have recently been reported. Jones *et al.* investigated the propensity of model proteins to aggregate in the presence of Si-oil and found that all the proteins tested aggregated in the presence of 0.5% Si-oil irrespective of molecular weight and isoelectric point of the protein (7). Thirumangalathu *et al.* studied Si-oil induced aggregation of an IgG1 monoclonal antibody as a function of agitation, temperature, pH, ionic strength, and excipient levels such as polysorbate 20 and sucrose. Although agitation-induced

aggregation was observed at higher speeds, addition of polysorbate 20 inhibited the aggregate formation (8). Overcashier *et al.* described some technical considerations for development of protein therapeutics in PFS including selection of primary components such as plungers and needle shields based on syringe functionality experiments (1).

In this paper, we have provided general guidance on the development of biotechnology products in PFS. We have systematically evaluated the effect of Si-oil on the compatibility of a mAb formulation through spiking studies and accelerated temperature stability studies. A study to compare two types of syringe barrels differentiated by the siliconization process has been presented. Furthermore, a strategy for screening primary components has been provided for determining optimum primary components for PFS systems.

## MATERIALS AND METHODS

### Materials

An in-house IgG2 mAb solution at 5 or 10 mg/mL in a buffer system at pH 6.0 containing surfactant and a disaccharide as excipients was used as a model protein formulation for this study. Si-oil (Dimethicone, 350 cs) was purchased from Dow Corning, Midland, MI, USA. The vials and syringes used in the study were made up of type I glass. Syringes were sourced from multiple vendors each using different processing methodologies to process and siliconize the barrels. Elastomeric closure components which can be sterilized by autoclaving (plungers) or ETO sterilization (tip caps) were used in this study. These were sourced from multiple vendors and are free of natural rubber and molded from standard formulations that meet requirements of the major pharmacopoeias.

### Silicone Oil–Water Emulsion Preparation

A stock solution of silicone oil/water emulsion was prepared as described earlier by Jones *et al.* (7). Si-oil was added in deionized water in a 50-mL centrifuge tube to obtain Si-oil concentration in water of 30 mg/mL. This solution was sonicated (Misonix S-4000) for approximately 5 min at 50% amplitude to obtain the emulsion which was opalescent due to fine dispersed Si-oil droplets. The stock solution was diluted to obtain emulsions at concentrations of 10 and 20 mg/mL Si-oil in water. The freshly prepared solutions were used to spike Si-oil into the mAb formulations.

### Agitation and Real-Time Stability Study Setup for the Spiked Samples

Type 1 glass vials (2 mL) were filled with 1 mL of the mAb formulation at 10 mg/mL and were spiked with 0.5, 1.0, or 1.5 mg equivalent of Si-oil. A control arm containing vials that were not spiked with Si-oil was included. The vials were placed in a box in the horizontal orientation to maximize the air–water interface. The boxes were then placed on orbital shakers at 5°C and room temperature and agitated at 300 rpm for 5 and 3 days, respectively. A vial from each group (control, 0.5, 1.0, and 1.5 mg/mL Si-oil) was removed after days 1, 2, and 3 at room temperature and after days 1, 3, and



5 at 5°C. In addition to the agitation stress study, a separate real-time and accelerated temperature stability study at 25°C and 40°C was initiated for vials that were spiked with the various levels of Si-oil. All stability vials were placed in the inverted orientation to maximize contact with the closure as a worse-case scenario.

### Stability Study Using Pre-filled Syringes

Two types of syringes, each with a different processing method, were used. The first type of syringe used was a luer-tip syringe with baked-on silicone. This syringe was subjected to a “baking” process post-siliconization wherein the syringes are exposed to a specific temperature for an appropriate time resulting in longer chains of Si that are more closely adhered to the surfaces they coat, thus resulting in a reduced concentration of free silicone in these syringes and lower chemical reactivity (9). The second type of syringe evaluated was one with the staked-in needle with silicone sprayed-on. The mAb formulations were filled into these syringes with a nominal fill of 1 mL, and plungers were placed using vacuum stoppering resulting in minimal (<1 mm) headspace between the liquid and the plunger. Syringes were then placed on real-time and accelerated temperature stability at 5°C, 25°C, and 40°C. All stability syringes were placed in the horizontal orientation to maximize contact with both the tip cap as well as the plunger stopper. For the purpose of this study, the two different types of syringes are referred to as baked-on or sprayed-on, respectively, in the “RESULTS” and “DISCUSSION” sections.

### Tip Cap Compatibility

Three different tip cap materials from two vendors were used in this study. An accelerated stability study at 25°C was initiated to discern the difference between tip cap materials and any potential effect on the stability of the mAb. Formulations at 5 mg/mL were used for this study. Each tip cap was cut into four pieces and added to a vial containing 1 mL of the mAb formulation. The surface area-to-volume ratio of the tip cap area exposed to liquid in the vial was kept constant for all three tip caps. A control arm was also added to the study where no tip cap material was added to the vials.

### Analytical Methods for Analysis

Protein concentration was calculated by using the extinction coefficient of the mAb and measuring the UV absorbance at 240 nm using a Cary 400 UV spectrophotometer (Agilent Technologies, Santa Clara, CA, USA). Formation of soluble aggregates was measured by SEC-HPLC using an Agilent 1100 system equipped with G3000SWXL and G2000SWXL columns in series. The detection wavelength was 214 nm using a diode array detector and a nominal protein concentration of 1 mg/mL. The protein was eluted isocratically with a 200-mM sodium phosphate (pH 7.0) mobile phase at a flow rate of 0.7 mL/min. Oxidation was assessed using a product-specific reversed-phase HPLC using an Agilent 1100 system equipped with two C18 columns in series. Enzymatic digestion was used to digest the mAb, and the met-256 containing fragment and its oxidized counterpart

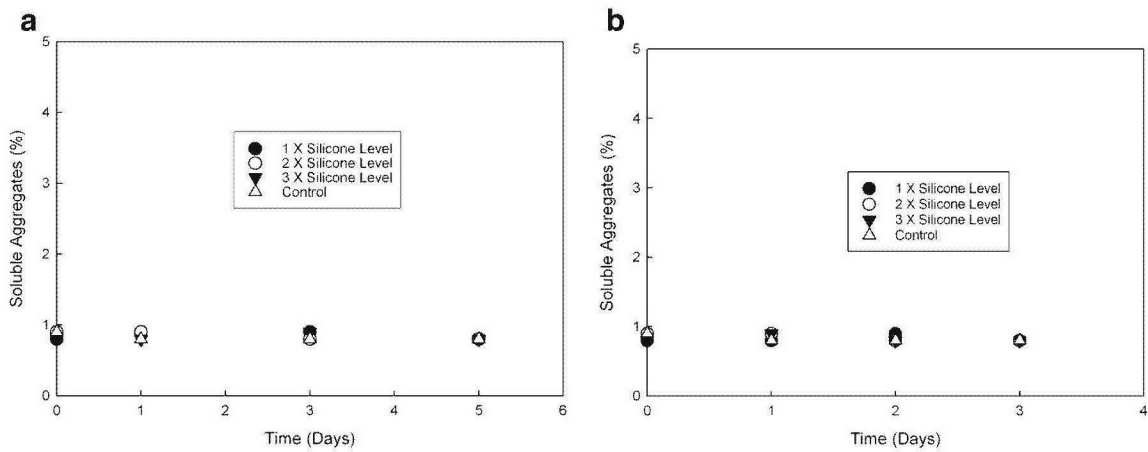
were monitored at 214 nm using a diode array detector and a nominal protein concentration of 1 mg/mL. All the aforementioned analytical assay methods had been validated specifically for the mAb that was studied. Subvisible particle analysis was performed using a HIAC 9703 equipped with an HRLD-150 sensor. A 15- $\mu$ m Duke latex count standard was run as a system suitability check prior to any sample analysis. In addition, a water blank was analyzed before each sample to ensure the background counts were appropriate for testing. All samples were equilibrated to room temperature before analysis.

## RESULTS

The aim of this report was to highlight the issues we experienced and approaches we took when developing a mAb product in PFS presentation. This should also provide some recommendations on approaches that can be used for development of similar products in PFS.

### Silicone Oil Compatibility: Spiking Approach

Si-oil levels typically observed (based on input from multiple syringe manufacturers) for staked-in needle syringes (0.5 to 0.8 mg/mL) were used for this study as a realistic representation of Si-oil. The mAb solution was spiked with stock Si-oil emulsion to achieve 0.5, 1.0, and 1.5 mg/mL silicone oil in mAb formulation as described in the “MATERIALS AND METHODS” section. These samples were subjected to an agitation stress study and a real-time and accelerated temperature stability study. A control arm consisting of formulations that were not spiked was also included in the study. The results for agitation stress study are shown in Fig. 1a, b for 5°C and 25°C, respectively. Soluble aggregate levels as measured by SEC did not show any appreciable difference when compared with control at 5°C and 25°C for up to 5 and 3 days, respectively, at an agitation speed of 300 rpm. Furthermore, no differences in appearance, protein concentration, or pH were observed. The stability study results, presented in Fig. 2a, b, show no significant change in soluble aggregate levels as a function of time and silicone oil spiking levels at 5°C. At the accelerated temperature condition of 25°C, a slight increase in soluble aggregates over 12 months was observed. Varying Si-oil spiking levels did not impact rate of formation of soluble aggregates. At 5°C, there was no observed increase in soluble aggregates even after 1 year of storage irrespective of silicone oil spiking level. In addition, no changes in color, clarity, pH, and protein concentration were observed over the duration of the study at either of the two temperatures for all the arms including control. All of the Si-oil spiked samples stored at 25°C had visible particle formation at the 1-year time point. This was also seen for samples spiked at the 1.5-mg Si-oil level at 5°C at the 1-year time point. No visible particle formation was observed for control samples at either temperature. Further investigation and particle characterization using a combination of optical microscopy (polarized light) and Fourier transform infrared spectroscopy (FTIR) was conducted. Results from optical microscopy are shown in Fig. 3. The particle morphology and



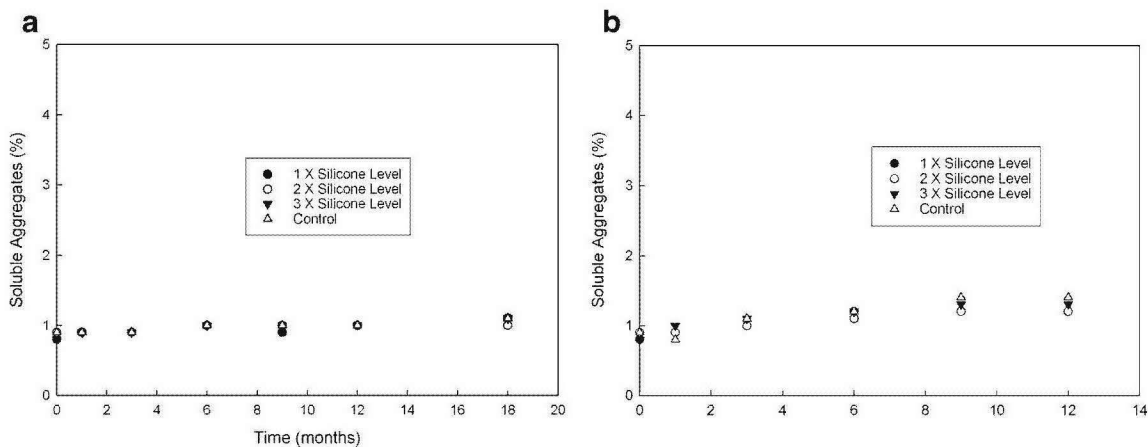
**Fig. 1.** Soluble aggregate levels for silicone oil spiked samples when subjected to agitation stress at **a** 5°C and **b** 25°C, respectively

reflectivity/opacity properties under varying light conditions suggest that the particles seen for samples at 25°C are a mixture of Si-oil droplets along with very small amorphous particles that resemble protein particulate matter. The shape and morphology of the silicone oil droplet observed was similar to that reported by Narhi *et al.* (10). Further characterization of these particles using FTIR spectroscopy confirmed that the amorphous particles observed were proteinaceous in nature. It can be hypothesized that, in the presence of Si-oil, prolonged exposure to accelerated temperature conditions has the potential to cause small amounts of protein to precipitate on the Si-oil droplets resulting in visible particles containing Si-oil and protein matter (Si-protein particle). It is important to note that the formation of these visible particles did not have significant impact on either protein concentration or soluble aggregate formation, indicating that the amount of protein precipitating was very small and within the assay variation for the concentration assay and that the formation of soluble aggregates was independent of the amount of Si-oil in the sample. Particle characterization of samples stored at 5°C, which had visible particle formation at the 1-year time point, indicated that they were Si-oil droplets without the presence of any protein-related matter. This suggests that samples containing high levels of Si-oil may be challenging for visual inspection due to the potential for

the Si-oil to coalesce over time resulting in higher levels of rejects of the drug product.

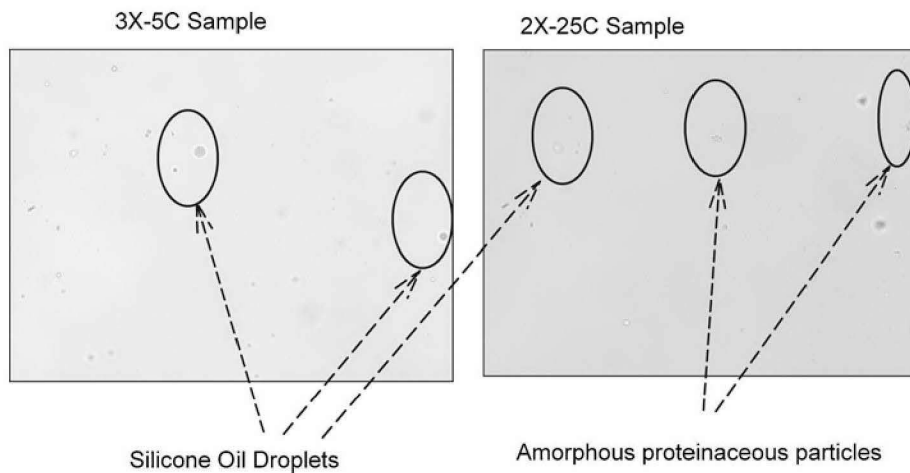
### Selection of Primary Components: Type of Syringe Barrel and Siliconization Process

The selection of primary components such as syringe barrel, plunger, and tip cap and/or needle shield is an important decision from a container closure standpoint. Oftentimes, several options are available, and it is important to choose the right combination of primary packaging material that can provide adequate stability for the molecule of interest as well as maintain the desired functionality properties over the product shelf life. This section highlights a study we conducted for choosing the correct type of syringe barrel for a mAb product. Two types of syringes, each with a different processing method, were used as described in the “METHODS AND MATERIALS” section. Real-time and accelerated temperature studies of the model mAb formulation in PFS were initiated. Based on extraction studies performed in our labs (data not shown), it was determined that the sprayed-on syringes contained higher residual-free silicone compared to baked-on silicone syringes. Figure 4a–c depicts soluble aggregate levels obtained for the 10-mg/mL mAb formulation stored in either sprayed-on or baked-on syringes at 5°C, 25°C, or 40°C, respectively. No specific trends



**Fig. 2.** Soluble aggregate levels for silicone oil spiked samples at **a** 5°C and **b** 25°C, respectively, when subjected to real-time and accelerated temperature conditions, as a function of time

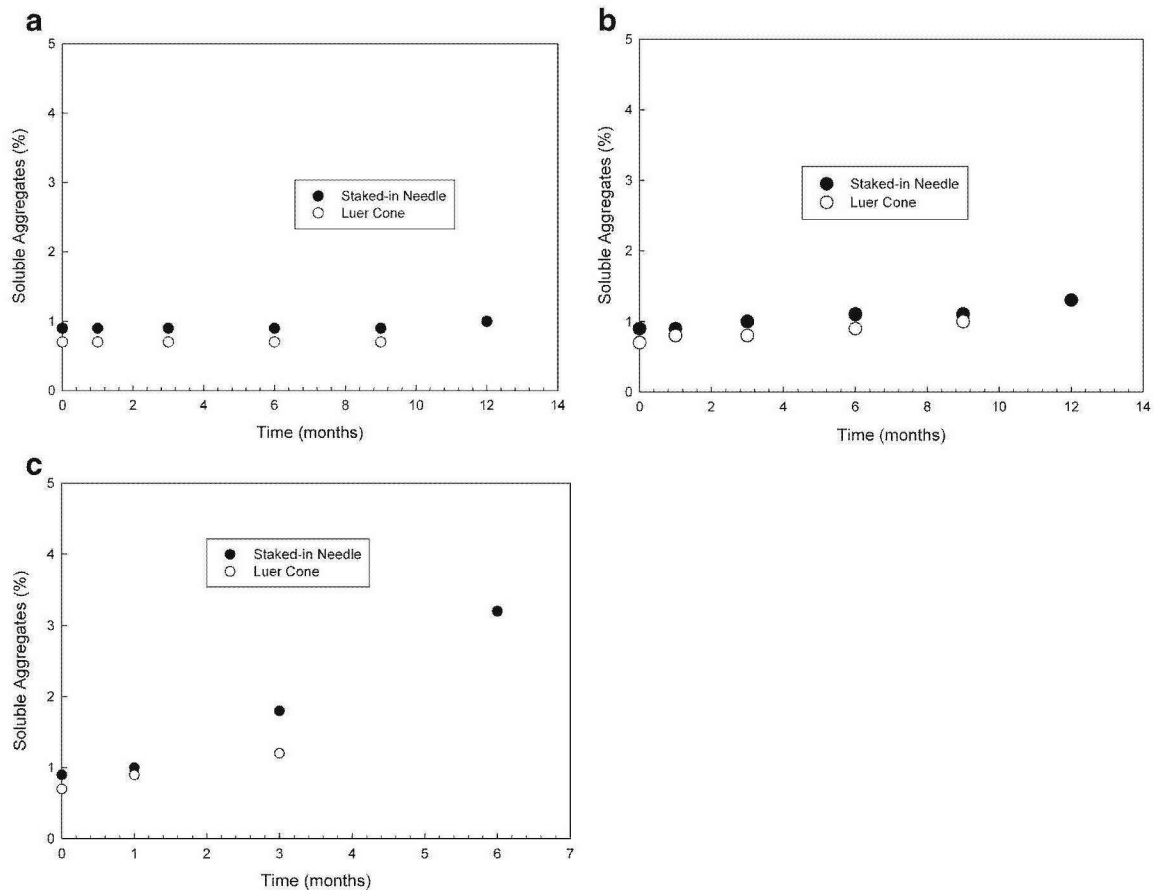




**Fig. 3.** Optical microscopy photographs showing silicone oil droplets and amorphous proteinaceous particles for 25°C sample spiked with 1 mg silicone oil and only silicone oil droplets for 5°C samples spiked with 1.5 mg silicone oil spiking

were observed in the stability profiles for both syringe types in the case of samples that were stored at 5°C, although a slight increase in soluble aggregate level was observed for the sprayed-on syringes stored at the accelerated temperature condition of 25°C. At 40°C, a significant increase in soluble aggregate formation was observed for the sprayed-on syringes. All the samples were visually free of particulate matter. In addition to this, the samples were evaluated for subvisible particle counts per USP <788> at both 5°C and 25°

C. For this assay, in addition to the USP-specified channels of 10 and 25 µm, particle counts at lower size-range channels such as 2, 5, and 8 µm were also measured to gather additional information in order to determine trends. As expected, the results from the subvisible particulate analysis on samples stored in baked-on syringes were within the USP <788> limits for 10 and 25 µm, and no specific trends were observed at the lower size channels as a function of time (Fig. 5a). Subvisible particle count levels for sprayed-on



**Fig. 4.** Soluble aggregate levels for sprayed-on and baked-on syringes at **a** 5°C, **b** 25°C, and **c** 40°C as a function of time

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