

US005654010A

Patent Number:

Date of Patent:

5,654,010 Aug. 5, 1997

Johnson et al.

[54] COMPOSITION FOR SUSTAINED RELEASE OF HUMAN GROWTH HORMONE

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- [21] Appl. No.: 473,544
- [22] Filed: Jun. 7, 1995

Related U.S. Application Data

- [63] Continuation-in-part of Ser. No. 984,323, Dec. 2, 1992, abandoned.
- [51] Int. Cl.⁶ A61F 2/02; A61K 9/14; A61K 9/50; A61K 38/24

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[57] ABSTRACT

A composition, and methods of forming and using said composition, for the sustained release of biologically active, stabilized human growth hormone (hGH). The sustained release composition of this invention comprises a polymeric matrix of a biocompatible polymer and particles of biologically active, stabilized hGH, wherein said particles are dispersed within the biocompatible polymer. The method of the invention for producing a composition for the sustained release of biologically active hGH, includes dissolving a biocompatible polymer in a polymer solvent to form a polymer solution, dispersing particles of biologically active, stabilized hGH in the polymer solution, and then solidifying the polymer to form a polymeric matrix containing a dispersion of said hGH particles. The method for using a composition of the invention is a method for providing a therapeutically effective blood level of biologically active, non-aggregated hGH in a subject for a sustained period. In this method, a subject is administered an effective dose of the sustained release composition of the present invention. The method of using the sustained release composition of the present invention comprises providing a therapeutically effective blood level of biologically active, non-aggregated human growth hormone in a subject for a sustained period by administering to the subject a dose of said sustained release composition.

11 Claims, No Drawings

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COMPOSITION FOR SUSTAINED RELEASE OF HUMAN GROWTH HORMONE

RELATED APPLICATIONS

This application is a Continuation-in-Part of U.S. patent application Ser. No. 07/984,323, filed Dec. 2, 1992, now abandoned, which is incorporated herein by reference in its entirety.

BACKGROUND OF THE INVENTION

Human growth hormone (hGH) is a protein secreted by the pituitary gland and which can be produced by recombinant genetic engineering. hGH will cause growth in all bodily tissues which are capable of growth.

hGH is typically used to treat patients suffering from hypopituitary dwarfism. Currently, aqueous hGH is administered as a subcutaneous bolus three times a week or once daily to patients to maintain suitable serum levels of hGH. For patients chronically receiving hGH, the frequent injec-²⁰ tions result in patient compliance problems.

To resolve the problems associated with repetitive injections of aqueous hGH, attempts have been made to formulate controlled release devices containing higher doses of hGH than a bolus injection, encapsulated within a polymeric matrix wherein the hGH would be released in vivo over a period of about a week or more.

However, these controlled release devices often exhibited high initial bursts of hGH release and minimal hGH release thereafter. Further, due to the high concentration of hGH within these controlled release devices, the hGH molecules have tended to aggregate after several days to form aggregated hGH which is immunogenic in vivo and likely has reduced biological activity. 35

Therefore, a need exists for a means for sustaining the release of biologically active hGH in vivo without causing an immune system response over the release period of the hGH.

SUMMARY OF THE INVENTION

This invention relates to a composition, and methods of forming and using said composition, for the sustained release of biologically active, stabilized human growth hormone (hGH). The sustained release composition of this invention comprises a polymeric matrix of a biocompatible polymer and particles of biologically active, stabilized hGH, wherein said particles are dispersed within the biocompatible polymer.

The method of the invention for forming a composition for the sustained release of hGH, includes dissolving a biocompatible polymer in a polymer solvent to form a polymer solution, dispersing particles of biologically active, stabilized hGH in the polymer solution, and then solidifying the polymer to form a polymeric matrix containing a dispersion of said hGH particles.

The method of using the sustained release composition of the present invention comprises providing a therapeutically effective blood level of biologically active, non-aggregated 60 human growth hormone in a subject for a sustained period by administering to the subject a dose of said sustained release composition.

The advantages of this sustained release formulation for hGH include longer, more consistent in vivo blood levels of 65 hGH, lower initial bursts of hGH, and increased therapeutic benefits by eliminating fluctuations in serum hGH levels.

The advantages also include increased patient compliance and acceptance by reducing the required number of injections. The advantages further include the ability to use smaller amounts of hGH compared to bolus injection regimen because serum hGH levels are maintained closer to therapeutical thresholds.

DETAILED DESCRIPTION OF THE INVENTION

The human growth hormone (hGH) used in this invention is biologically active hGH in its molecular (monomeric or non-aggregated) form. Molecular hGH is typically nonimmunogenic.

Aggregated hGH may induce an immune response resulting in antibodies formed against hGH. This may compromise the efficacy of long-term hGH therapy. Additionally, aggregated hGH may stimulate an auto-immune response to endogenous hGH.

A sustained release of biologically active, non-aggregated human growth hormone is a release which results in measurable serum levels of biologically active, monomeric hGH over a period longer than that obtained following direct administration of aqueous hGH. It is preferred that a sustained release be a release of hGH for a period of about a week or more, and more preferably for a period of about two weeks or more.

A sustained release of biologically active, non-aggregated hGH from a polymeric matrix can be continuous or non-³⁰ continuous release with relatively constant or varying rates of release. The continuity of hGH released and level of hGH released can be established by using, inter-alia, one or more types of polymer compositions, hGH loadings, and/or selection of excipients to produce the desired effect.

Stabilized (hGH) comprises biologically active, nonaggregated hGH which is complexed with at least one type of multivalent metal cation, having a valency of +2 or more, from a metal cation component. Stabilized hGH in the sustained release composition of the present invention is in particulate form.

Suitable multivalent metal cations include metal cations contained in biocompatible metal cation components. A metal cation component is biocompatible if the cation component is non-toxic to the recipient, in the quantities used, and also presents no significant deleterious or untoward effects on the recipient's body, such as an immunological reaction at the injection site.

Typically, the molar ratio of metal cation component to $_{50}$ hGH, for the metal cation stabilizing the hGH, is between about 4:1 to about 10:1.

A preferred metal cation used to stabilize hGH is Zn^{+2} . In a more preferred embodiment, the molar ratio of metal cation component, containing Zn^{+2} cations, to hGH is about 6:1.

The suitability of a metal cation for stabilizing hGH can be determined by one of ordinary skill in the art by performing a variety of stability indicating techniques such as polyacrylamide gel electrophoresis, isoelectric focusing, reverse phase chromatography, HPLC and potency tests on hGH lyophilized particles containing metal cations to determine the potency of the hGH after lyophilization and for the duration of release from microparticles. In stabilized hGH, the tendency of hGH to aggregate within a microparticle during hydration in vivo and/or to lose biological activity or potency due to hydration or due to the process of forming a sustained release composition, or due to the chemical char5

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acteristics of a controlled release composition, is reduced by complexing at least one type of metal cation with hGH prior contacting the hGH with a polymer solution.

Stabilized hGH is typically stabilized against significant aggregation in vivo over the sustained release period.

Stabilized hGH is typically stabilized against significant aggregation in vivo over the sustained release period. Significant aggregation is defined as an amount of aggregation resulting in aggregation of about 15% or more of the initial amount of encapsulated hGH monomer. Preferably, aggre-¹⁰ gation is maintained below about 5% of the initial dose of hGH monomer. More preferably, aggregation is maintained below about 2% of the initial dose.

The hGH in a hGH sustained release composition can also be mixed with other excipients, such as bulking agents or ¹⁵ additional stabilizing agents, such as buffers to stabilize the hGH during lyophilization.

Bulking agents typically comprise inert materials. Suitable bulking agents are known to those skilled in the art.

A polymer, or polymeric matrix, suitable for the sustained release composition of the present invention must be biocompatible. A polymer is biocompatible if the polymer, and any degradation products of the polymer, are non-toxic to the recipient and also present no significant deleterious or untoward effects on the recipient's body, such as an immunological reaction at the injection site.

The polymer of the hGH sustained release composition must also be bidegradable. Biodegradable as defined herein, means the composition will degrade or erode in vivo to form smaller chemical species. Degradation can result, for example, by enzymatic, chemical and physical processes. Suitable biocompatible, biodegradable polymers include, for example, poly(lactides), poly(glycolides), poly(lactide-coglycolides), poly(lactic acid)s, poly(glycolic acid)s, poly (lactic acid-co-glycolic acid)s, polycaprolactone, polycarbonates, polyesteramides, polyanhydrides, poly (amino acids), poly(alkylene oxalate)s, biodegradable polyurethanes, blends and copolymers thereof. 40

Further, the terminal functionalities of the polymer can be modified. For example, polyesters can be blocked, unblocked or a blend of blocked and unblocked polymers. A blocked polymer is as classically defined in the art, specifically having blocked carboxyl end groups. Generally, the 45 blocking group is derived from the initiator of the polymerization and is typically an alkyl group. An unblocked polymer is as classically defined in the art, specifically having free carboxyl end groups.

Acceptable molecular weights for polymers used in this 50 invention can be determined by a person of ordinary skill in the art taking into consideration factors such as the desired polymer degradation rate, physical properties such as mechanical strength, and rate of dissolution of polymer in solvent. Typically, an acceptable range of molecular weights 55 is of about 2,000 Daltons to about 2,000,000 Daltons. In a preferred embodiment, the polymer is a biodegradable polymer or copolymer. In a more preferred embodiment, the polymer is a poly(lactide-co-glycolide) (hereinafter "PLGA") with a lactide: glycolide ratio of about 1:1 and a 60 molecular weight of about 5,000 Daltons to about 70,000 Daltons. In an even more preferred embodiment, the molecular weight of the PLGA used in the present invention has a molecular weight of about 6,000 to about 31,000 Daltons.

The amount of hGH, which is contained in a dose of sustained release microparticles, or in an alternate sustained

release device, containing biologically active, stabilized hGH particles is a therapeutically or prophylactically effective amount, which can be determined by a person of ordinary skill in the art taking into consideration factors such as body weight, condition to be treated, type of polymer used, and release rate from the polymer.

In one embodiment, an hGH sustained release composition contains from about 0.01% (w/w) to about 50% (w/w) of biologically active, stabilized hGH particles. The amount of such hGH particles used will vary depending upon the desired effect of the hGH, the planned release levels, the times at which hGH should be released, and the time span over which the hGH will be released. A preferred range of hGH particle loading is between about 0.1% (w/w) to about 30% (w/w) hGH particles. A more preferred range of hGH particle loading is between about 0.1% (w/w) to about 20% (w/w) hGH particles. The most preferred loading of the biologically active, stabilized hGH particles is about 15% (w/w).

In another embodiment, a hGH sustained release composition also contains a second metal cation component, which is not contained in the stabilized hGH particles, and which is dispersed within the polymer. The second metal cation component preferably contains the same species of metal cation, as is contained in the stabilized hGH. Alternately, the second metal cation component can contain one or more different species of metal cation.

The second metal cation component acts to modulate the release of the hGH from the polymeric matrix of the sustained release composition, such as by acting as a reservoir of metal cations to further lengthen the period of time over which the hGH is stabilized by a matal cation to enhance the stability of hGH in the composition.

A metal cation component used in modulating release typically contains at least one type of multivalent metal cation. Examples of second metal cation components suitable to modulate hGH release, include, or contain, for instance, Mg(OH)₂, MgCO₃ (such as 4MgCO₃.Mg(OH) $_2.5H_2O$), ZnCO₃ (such as 3Zn(OH) $_2.2ZnCO_3$), CaCO₃, Zn₃ (C₆H₅O₇)₂, Mg(OAc)₂, MgSO₄, Zn(OAc)₂, ZnSO₄, ZnCl₂, MgCl₂ and Mg₃(C₆H₅O₇)₂. A suitable ratio of second metal cation component-to-polymer is between about 1:99 to about 1:2 by weight. The optimum ratio depends upon the polymer and the second metal cation component utilized.

A polymeric matrix containing a dispersed metal cation component to modulate the release of a biologically active agent from the polymeric matrix is further described in co-pending U.S. patent application Ser. No. 08/237,057, filed May 3, 1994, and co-pending PCT Patent Application PCT/US95/05511, the teachings of which are incorporated herein by reference in their entirety.

The hGH sustained release composition of this invention can be formed into many shapes such as a film, a pellet, a cylinder, a disc or a microparticle. A microparticle, as defined herein, comprises a polymeric component having a diameter of less than about one millimeter and having stabilized hGH particles dispersed therein. A microparticle can have a spherical, non-spherical or irregular shape. It is preferred that a microparticle be a microsphere. Typically, the microparticle will be of a size suitable for injection. A preferred size range for microparticles is from about 1 to about 180 microns in diameter.

In the method of this invention for forming a composition for the sustained release of biologically active, non-65 aggregated hGH, a suitable amount of particles of biologically active, stabilized hGH are dispersed in a polymer solution 5

A suitable polymer solution contains between about 1% (w/w) and about 30% (w/w) of a suitable biocompatible polymer, wherein the biocompatible polymer is typically dissolved in a suitable polymer solvent. Preferably, a polymer solution contains about 2% (w/v) to about 20% (w/v) polymer. A polymer solution containing 5% to about 10% (w/w) polymer is most preferred.

A suitable polymer solvent, as defined herein, is solvent in which the polymer is soluble but in which the stabilized hGH particles are substantially insoluble and non-reactive. 10 Examples of suitable polymer solvents include polar organic liquids, such as methylene chloride, chloroform, ethyl acetate and acetone.

To prepare biologically active, stabilized hGH particles, hGH is mixed in a suitable aqueous solvent with at least one 15 suitable metal cation component under pH conditions suitable for forming a complex of metal cation and hGH.

Suitable pH conditions to form a complex of hGH typically include pH values between about 7.0 and about 7.4. Suitable pH conditions are typically achieved through use of an aqueous buffer, such as sodium bicarbonate, as the 20 solvent.

Suitable solvents are those in which the hGH and the metal cation component are each at least slightly soluble, such as in an aqueous sodium bicarbonate buffer. For 25 aqueous solvents, it is preferred that water used be either deionized water or water-for-injection (WFI).

It is understood that the hGH can be in a solid or a dissolved state, prior to being contacted with the metal cation component. It is also understood that the metal cation $_{30}$ component can be in a solid or a dissolved state, prior to being contacted with the hGH. In a preferred embodiment, a buffered aqueous solution of hGH is mixed with an aqueous solution of the metal cation component.

Typically, the complexed hGH will be in the form of a 35 cloudy precipitate, which is suspended in the solvent. However, the complexed hGH can also be in solution. In an even more preferred embodiment, hGH is complexed with Zn^{+2} .

The complexed hGH is then dried, such as by 40 lyophilization, to form a particulate of stabilized hGH. The complexed hGH, which is suspended or in solution, can be bulk lyophilized or can be divided into smaller volumes which are then lyophilized. In a preferred embodiment, the complexed hGH suspension is micronized, such as by use of 45 an ultrasonic nozzle, and then lyophilized to form stabilized hGH particles. Acceptable means to lyophilize the complexed hGH mixture include those known in the art.

Preferably, particles of stabilized hGH are between about 1 to about 6 micrometers in diameter. The hGH particles can 50 be fragmented separately, as described in co-pending U.S. patent application Ser. No. 08/006,682, filed Jan. 21, 1993, which describes a process for producing small particles of biologically active agents, which is incorporated herein in its entirety by reference. Alternately, the hGH particles can be 55 solid and/or liquid into the non-solvent to form stabilized fragmented after being added to a polymer solution, such as by means of an ultrasonic probe or ultrasonic nozzle. In another embodiment, a second metal cation component, which is not contained in the stabilized hGH particles, is also dispersed within the polymer solution.

It is understood that a second metal cation component and stabilized hGH can be dispersed into a polymer solution sequentially, in reverse order, intermittently, separately or through concurrent additions. Alternately, a polymer, a second metal cation component and stabilized hGH and can be 65 mixed into a polymer solvent sequentially, in reverse order, intermittently, separately or through concurrent additions.

The method for forming a composition for modulating the release of a biologically active agent from a biodegradable polymer is further described in co-pending U.S. patent application Ser. No. 08/237,057.

In this method, the polymer solvent is then solidified to form a polymeric matrix containing a dispersion of stabilized hGH particles.

One suitable method for forming an hGH sustained release composition from a polymer solution is the solvent evaporation method described in U.S. Pat. No. 3,737,337, issued to Schnoring et al., U.S. Pat. No. 3,529,906, issued to Vranchen et al., U.S. Pat. No. 3,691,090, issued to Kitajima et al., or U.S. Pat. No. 4,389,330, issued to Tice et al. Solvent evaporation is typically used as a method to form hGH sustained release microparticles.

In the solvent evaporation method, a polymer solution containing a stabilized hGH particle dispersion, is mixed in or agitated with a continuous phase, in which the polymer solvent is partially miscible, to form an emulsion. The continuous phase is usually an aqueous solvent. Emulsifiers are often included in the continuous phase to stabilize the emulsion. The polymer solvent is then evaporated over a period of several hours or more, thereby solidifying the polymer to form a polymeric matrix having a dispersion of stabilized hGH particles contained therein.

A preferred method for forming hGH sustained release microparticles from a polymer solution is described in U.S. Pat. No. 5,019,400, issued to Gombotz et al., and co-pending U.S. patent application Ser. No. 08/443,726, filed May 18, 1995, the teachings of which are incorporated herein by reference in their entirety. This method of microsphere formation, as compared to other methods, such as phase separation, additionally reduces the amount of hGH required to produce a controlled release composition with a specific hGH content.

In this method, the polymer solution, containing the stabilized hGH particle dispersion, is processed to create droplets, wherein at least a significant portion of the droplets contain polymer solution and the stabilized hGH particles. These droplets are then frozen by means suitable to form microparticles. Examples of means for processing the polymer solution dispersion to form droplets include directing the dispersion through an ultrasonic nozzle, pressure nozzle, Rayleigh jet, or by other known means for creating droplets from a solution.

Means suitable for freezing droplets to form microparticles include directing the droplets into or near a liquified gas, such as liquid argon and liquid nitrogen to form frozen microdroplets which are then separated from the liquid gas. The frozen microdroplets are then exposed to a liquid non-solvent, such as ethanol, or ethanol mixed with hexane or pentane.

The solvent in the frozen microdroplets is extracted as a hGH containing microparticles. Mixing ethanol with other non-solvents, such as hexane or pentane, can increase the rate of solvent extraction, above that achieved by ethanol alone, from certain polymers, such as poly(lactide-co-60 glycolide) polymers.

A wide range of sizes of hGH sustained release microparticles can be made by varying the droplet size, for example, by changing the ultrasonic nozzle diameter. If very large microparticles are desired, the microparticles can be extruded through a syringe directly into the cold liquid. Increasing the viscosity of the polymer solution can also increase microparticle size. The size of the microparticles

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can be produced by this process, for example microparticles ranging from greater than about 1000 to about 1 micrometers in diameter.

Yet another method of forming an hGH sustained release composition, from a polymer solution, includes film casting, 5 such as in a mold, to form a film or a shape. For instance, after putting the polymer solution containing a dispersion of stabilized hGH particles into a mold, the polymer solvent is then removed by means known in the art, or the temperature of the polymer solution is reduced, until a film or shape, with 10 a consistent dry weight, is obtained. Film casting of a polymer solution, containing a biologically active agent, is further described in co-pending U.S. patent application Ser. No. 08/237,057, the teachings of which are incorporated herein by reference in their entirety. 15

It is believed that the release of the hGH can occur by two different mechanisms. The hGH can be released by diffusion through aqueous filled channels generated in the polymeric matrix, such as by the dissolution of the hGH or by voids created by the removal of the polymer's solvent during the 20 synthesis of the sustained release composition. A second mechanism is the release of hGH due to degradation of the polymer.

The rate of degradation can be controlled by changing 25 polymer properties that influence the rate of hydration of the polymer. These properties include, for instance, the ratio of different monomers, such as lactide and glycolide, comprising a polymer; the use of the L-isomer of a monomer instead of a racemic mixture; and the molecular weight of the 30 polymer. These properties can affect hydrophilicity and crystallinity, which control the rate of hydration of the polymer. Hydrophilic excipients such as salts, carbohydrates and surfactants can also be incorporated to increase hydration and which can alter the rate of erosion of the polymer. 35

By altering the properties of the polymer, the contributions of diffusion and/or polymer degradation to hGH release can be controlled. For example, increasing the glycolide content of a poly(lactide-co-glycolide) polymer and decreasing the molecular weight of the polymer can enhance the hydrolysis of the polymer and thus, provides an increased hGH release from polymer erosion.

In addition, the rate of polymer hydrolysis is increased in non-neutral pH's. Therefore, an acidic or a basic excipient can be added to the polymer solution, used to form the 45 microsphere, to alter the polymer erosion rate.

The composition of this invention can be administered to a human, or other animal, by injection, implantation (e.g. subcutaneously, intramuscularly, intraperitoneally, intracranially, intravaginally and intradermally), administra- 50 tion to mucosal membranes (e.g., intranasally or by means of a suppository), or in situ delivery (e.g. by enema or aerosol spray) to provide the desired dosage of hGH based on the known parameters for treatment with hGH of the various medical conditions.

The invention will now be further and specifically described by the following examples.

EXAMPLE 1

Formation of Zn⁺²-Stabilized hGH

Human growth hormone (hGH), whose DNA sequence is described in U.S. Pat. No. 4,898,830, issued to Goeddel et al. was used in this Example. Human growth hormone was stabilized by forming an insoluble complexes with zinc. 65

The hGH was dissolved in Samples of a 4 mM sodium hicarhonate buffer (nH 7.2) to form hGH solutions with

concentrations between 0.1 and 0.5 mM hGH. A 0.9 mM Zn⁺² solution was prepared from deionized water and zinc acetate dihydrate and then was added to the hGH solutions to form a Zn^{+2} -hGH complex. The pH of the Zn^{+2} -hGH solution was then adjusted to between 7.0 and 7.4 by adding 1% acetic acid. A cloudy suspended precipitate, comprising Zn⁺²-stabilized hGH formed.

The suspension of Zn+2-stabilized hGH was then micronized using an ultrasonic nozzle (Type V1A; Sonics and Materials, Danbury, Conn.) and sprayed into a polypropylene tub (17 cm diameter and 8 cm deep) containing liquid nitrogen to form frozen particles. The polypropylene tub was then placed into a -80° C. freezer until the liquid nitrogen evaporated. The frozen particles, which contained Zn⁺²stabilized hGH, were then lyophilized to form Zn⁺²stabilized hGH particles.

EXAMPLE 2

Preparation of PLGA Microspheres Containing Biologically Active, Zn+2-Stabilized hGH

Microspheres containing Zn⁺²-stabilized human growth hormone (hGH), were prepared from hydrophilic poly (lactice-co-glycolide) polymer RG502H having free carboxyl end groups (hereinafter "unblocked-PLGA") (50:50 PLGA, 9,300 Daltons; Boehringer Ingelheim Chemicals, Inc.) or a more hydrophobic PLGA polymer having blocked carboxyl end groups (hereinafter "blocked-PLGA") (50:50 PLGA, 10,000 Daltons; Lot #115-56-1, Birmingham Polymers, Inc., Birmingham, Ala.).

The polymer was dissolved in methylene chloride at room temperature. The lyophilized hGH particles were added to the polymer solution and zinc carbonate was also added. The mixture was then sonicated to give a homogeneous suspension. The suspension was atomized through a sonicating nozzle on to a bed of frozen ethanol, overlaid with liquid nitrogen. The vessel containing the microspheres was stored at -80° C. to extract the methylene chloride and then 40 freeze-dried to give a free-flowing powder.

EXAMPLE 3

Analysis of Encapsulated hGH Protein

The integrity of encapsulated hGH was determined by dissolving unhydrated microspheres into methylene chloride and acetone, collecting the protein, freeze-drying and re-constituting in HEPES buffer containing 10 mM EDTA. Appropriate controls were run to ensure that the extraction process did not affect the integrity of the protein.

The integrity of the encapsulated hGH was analyzed by measuring the percent of hGH monomer contained in the hGH sample after encapsulation by size exclusion chromatography (SEC).

The results of SEC analyses of the hGH integrity of hGH sustained release microspheres are provided below.

60	Formulation (polymer; % Zinc Carbonate)	% Monomer (SEC)	
_	31K unblocked; 6% ZnCO3	98.6	
	31K unblocked; 6% ZnCO3	99.2	
	31K unblocked; 3% ZnCO3	97.7	
	31K unblocked; 3% ZnCO3	97.8	
	31K unblocked; 1% ZnCO3	97.6	
55	31K unblocked; 0% ZnCO3	97.8	
	31K unblocked: 0% ZnCO3	97.1	

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